

# ADOPTION OF THE ISO 5832-1 AUSTENITIC STAINLESS-STEEL TREATED BY OPTICAL FIBER LASER FOR BIOMEDICAL APPLICATIONS: A TRIBOLOGICAL BEHAVIOR ANALYSIS

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# ABSTRACT

The present work analyzed the influence of an optical fiber laser surface treatment process on the tribological behavior of the ISO 5832-1 austenitic stainless-steel, basing on the wear volume and coefficient of friction. Specimen of this biomaterial were treated by alternating the laser frequency, in order to find out a condition that improves its tribological resistance. Ball-cratering micro-abrasive wear tests were carried out with a test ball of AISI 316L austenitic stainless-steel, used as counter-body, and an abrasive slurry prepared with abrasive particles of black silicon carbide (SiC) and distilled water. The micro-abrasive wear tests results indicated that: i) the hardness of the ISO 5832-1 austenitic stainless-steel increased as a function of the laser frequency, decreasing, consequently, the wear volume, as predicted by Archard's Law, ii) the coefficient of friction did not present a proportional behavior with the increase of the optical fiber laser frequency and iii) the best condition to improve the wear resistance of the ISO 5832-1 austenitic stainless-steel an optical fiber laser frequency of 350 kHz, being reported the lower wear volume.

**Keywords:** Biomaterials, austenitic stainless-steel, optical fiber laser, micro-abrasive wear, tribological resistance.

### **INTRODUCTION**

Recently, the micro-scale abrasive wear test by rotating ball has gained large acceptance in universities and research centers, being widely used in studies on the micro-abrasive wear behavior of materials. Figure  $1a^{(1-3)}$  presents a schematic diagram of the principle of this micro-abrasive wear test, where a rotating test ball is forced against the tested specimen, in the presence of an abrasive slurry. There are two main test devices configurations to conduct this type of micro-abrasive wear test: "*free-ball*" and "*fixed-ball*" mechanical configurations; Figures  $1b^{(4,5)}$  and  $1c^{(6)}$  show examples of these experimental devices.





Figure 1: Micro-abrasive wear testing by rotating ball: (a) schematic diagram of its principle operating<sup>(1-3)</sup>, (b) "*free-ball*" mechanical configuration<sup>(4,5)</sup> and (c) "*fixed-ball*" mechanical configuration<sup>(6)</sup>; "*h*" is the wear crater depth and "*n*" is the test ball rotational speed.

The aim of the micro-abrasive wear test by rotating ball is to generate "*wear craters*" on the specimen. Figure 2 presents images of such craters, together with an indication of the crater diameter (*d*) and the wear volume  $(V)^{(7)}$ .

The wear volume (V) may be determined as a function of "d", using Equation  $A^{(8)}$ , where "R" is the radius of the test ball.

$$V \cong \frac{\pi d^4}{64R}$$
 for  $d \ll R$  (A)

The micro-abrasive wear test has been applied in the study of the micro-abrasive wear behavior of metallic<sup>(1,4,9-12)</sup> and non-metallic<sup>(2,3,13-19)</sup> materials and their wear behavior can be expressed based on the wear volume (*V*) and/or friction coefficient ( $\mu$ ), calculated from Equation B, where "*N*" is the normal force applied on the specimen and "*T*" is the tangential force measured during the wear tests (see Figure 1a).



Figure 2: Images of wear craters: (a) diameter -d and (b) wear volume  $-V^{(7)}$ .

Micro-abrasive wear tests conducted under the "*ball-cratering*" technique present advantages in relation to other types of wear tests, because it can be performed with normal forces (N) relatively low (N < 0.5 N) and, in principle, can favor the analysis of the tribological behavior that is desired.

In other hand, along the last years, the concept of "*biotribology*" has gained important spotlight in the area, including researches addressing the tribological behavior of human body elements. Then, different laboratory techniques and specialties have been employed to reproduce conditions where there are friction and consequent wear of parts of the mechanical structure human with relative movement.

In view of this important research line -biotribology – to people benefit, the purpose of this present work is to analyze the influence of an optical fiber laser surface treatment process on the tribological behavior of ISO 5832-1 austenitic stainless-steel, in order to find out a process condition that improves its wear resistance.

#### EXPERIMENTAL DETAILING

Micro-abrasive wear tests were conducted with a ball-cratering equipment of "*free-ball*" mechanical configuration (Figure 3).

Two load cells were used in the ball-cratering micro-abrasive wear test equipment: one load cell to control the normal force (*N*) applied on the specimen and one load cell to measure the tangential force (*T*) developed during the experiments. "*Normal*" and "*tangential*" force load cells have a maximum capacity of  $\Gamma = 50$  N, an accuracy of  $\Pi = 0.001$  N and the values of "*N*" and "*T*" appear on a readout system in real time during testing.



Figure 3: Ball-cratering equipment with "free-ball" mechanical configuration used for the microabrasive wear tests of this work.

Surfaces of ISO 5832-1 austenitic stainless-steel specimen were treated with three different frequencies of optical fiber laser (*f*):  $f_1 = 80$  kHz,  $f_2 = 296$  kHz and  $f_3 = 350$  kHz. After, Vickers Hardness tests were conducted on "*non-treated*" specimen and "*treated*" specimen with the different optical fiber laser frequencies.

The counter-body was a test ball of AISI 316L austenitic stainless-steel with diameter of  $D = 25.4 \text{ mm} (D = 1^{\circ}) - \text{standard size}$ .

Table 1 presents the micro-abrasive wear test conditions defined for the experiments.

Table 1: Micro-abrasive wear test conditions defined for the experiments.

Test parameter	Value
Normal force $-N$	0.5 N
Test ball rotational speed $-n$	70 rpm
Abrasive slurry concentration $-C$	5% SiC + 95% distilled water (in volume)
Sliding distance – S	25 m

The normal force value defined for the wear experiments was N = 0.5 N, together a test ball rotational speed of n = 70 rpm. The abrasive slurry was prepared with black silicon carbide (SiC) with average particle size of  $a_p = 3 \mu m$  and angular shape, under the concentration of C = 5% SiC + 95% distilled water (volumetric values – by literature<sup>(10)</sup>, this value of abrasive slurry concentration is considered relatively low). For all experiments, the total sliding distance stablished was S = 25 m.

The tribological behavior of "non-treated" and "treated by optical fiber laser" surfaces of ISO 5832-1 austenitic stainless-steel were analyzed based on the wear volume (V) and friction coefficient ( $\mu$ ).

#### **RESULTS AND DISCUSSION**

#### Results - Regarding to action of the "grooving abrasion" wear mode

Figure 4 presents a wear crater image, being possible to observe the occurrence of "grooving abrasion" wear mode, due to low abrasive slurry concentration defined for the micro-abrasive wear experiments of this research (C = 5% SiC + 95% distilled water – in volume).



Figure 4. Occurrence of "grooving abrasion" wear mode on the surface of a wear crater.

The action of "grooving abrasion" wear mode reported on the surfaces of the wear craters obtained in this work is in qualitative agreement with the conceptualization addressed in the classical work published by R.I. Trezona, D.N. Allsopp and I.M. Hutchings<sup>(10)</sup>, where is explained and demonstrated that low concentrations of abrasive slurries (< 25% abrasive material – in volume) favor the occurrence of "grooving abrasion" wear mode.

#### <u>Results</u> – Values of hardness (H), wear volume (V) and friction coefficient ( $\mu$ )

Table 2 shows the values of the hardness (*H*), wear volume (*V*) and friction coefficient ( $\mu$ ) obtained for the ISO 5832-1 austenitic stainless-steel surfaces, under conditions of "*non-treated*" and "*treated*" with the different optical fiber laser frequencies (*f*).

Table 2: Values of the hardness (*H*), wear volume (*V*) and friction coefficient ( $\mu$ ) reported for the specimen under the conditions of "*non-treated*" and "*treated*" with the different optical fiber laser frequencies (*f*).

Surface specimen treatment	Hardness – H [HV]	Wear volume – $V$ [ $10^{-3}$ mm <sup>3</sup> ]	<b>Friction coefficient</b> – μ
Non-treated	199	6.2	0.12
<i>Treated</i> $\Rightarrow$ $f_1 = 80 \text{ kHz}$	204	5.4	0.15
<i>Treated</i> $\Rightarrow$ $f_2 = 296$ kHz	226	4.4	0.10
<i>Treated</i> $\Rightarrow$ $f_3 = 350 \text{ kHz}$	240	3.7	0.14

It is possible to observe that the optical fiber laser frequency presented influence on the values of hardness, wear volume and friction coefficient.

#### Discussion - Regarding to tribological behavior of ISO 5832-1 austenitic stainless-steel

Analyzing the values of Table 1, it is possible to note that the hardness (*H*) increased with the increase of the optical fiber laser frequency (*f*), considering the condition of "*non-treated*" surface and the conditions of "*treated*" surfaces, where the laser frequency was varied from  $f_1 = 80$  kHz to  $f_3 = 350$  kHz.

Besides, due to increase of the hardness as a function of the optical fiber laser frequency – H = f(f), was reported a decrease of the wear volume (*V*), according qualitatively to *Archard's Law* (Equation C).

$$V = \xi \frac{S.N}{H} \tag{C}$$

Where  $\xi$  is a dimensionless constant that indicate the severity of the micro-abrasive wear process<sup>(20)</sup>.

In fact, by *Archard's Law*, the wear volume is inversely proportional to material hardness. Regarding to values of the friction coefficient ( $\mu$ ), they varied from  $\mu = 0.10$  to  $\mu = 0.15$  and they did not present a direct relationship with the hardness (*H*) of the specimen and/or with the wear volume (*V*).

Finally, the best condition of optical fiber laser frequency stablished for the surface treatment of the ISO 5832-1 austenitic stainless-steel was  $f_3 = 350$  kHz, because this laser frequency condition provided the lower value of wear volume –  $V_3 = 3.7 \times 10^{-3}$  mm<sup>3</sup>, featuring the higher micro-abrasive wear resistance.

### CONCLUSIONS

The results obtained in this research indicated that:

- (1) The hardness of the "*treated*" surface of the ISO 5832-1 austenitic stainless-steel was dependent of the optical fiber laser frequency value the material hardness increased with the increase of the laser frequency;
- (2) With the increase of the material hardness, the wear volume decreased, following, qualitatively, the *Archard's Law*, where the wear volume is inversely proportional to material hardness;
- (3) The friction coefficient did not present a proportional behavior with the increase of the optical fiber laser frequency and consequent increase of the material hardness, *i.e.*, was not observed a direct relationship between material hardness and friction coefficient;
- (4) The micro-abrasive wear results indicated that the tribological behavior was influenced by the frequencies values used for the laser surface treatment and the best condition to improve the wear resistance of ISO 5832-1 austenitic stainless-steel was obtained adopting an optical fiber laser frequency of 350 kHz, obtaining the lower wear volume.

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# LIST OF SYMBOLS – NOMENCLATURE AND UNITS

$a_p$	Average abrasive particle size	[µm]
С	Abrasive slurry concentration	[%SiC + % distilled water]
d	Diameter of the wear crater	[mm]
D	Diameter of the test ball	[mm]
f	Optical fiber laser frequency	[kHz]
h	Wear crater depth	[µm]
Η	Hardness	[HV]
n	Test ball rotational speed	[rpm]
N	Normal force	[N]
	(applied on the specimen)	
R	Radius of the test ball	[mm]
S	Sliding distance	[m]
Т	Tangential force	[N]
	(measured on the tribological system)	
V	Wear volume	[mm <sup>3</sup> ]
Greek	letters	
Γ	Maximum capacity of the load cells	[N]
μ	Friction coefficient	
Π	Accuracy of the load cells	[N]

 $\xi$  Dimensionless constant that indicate the severity of the micro-abrasive wear process – from *Archard's Law*